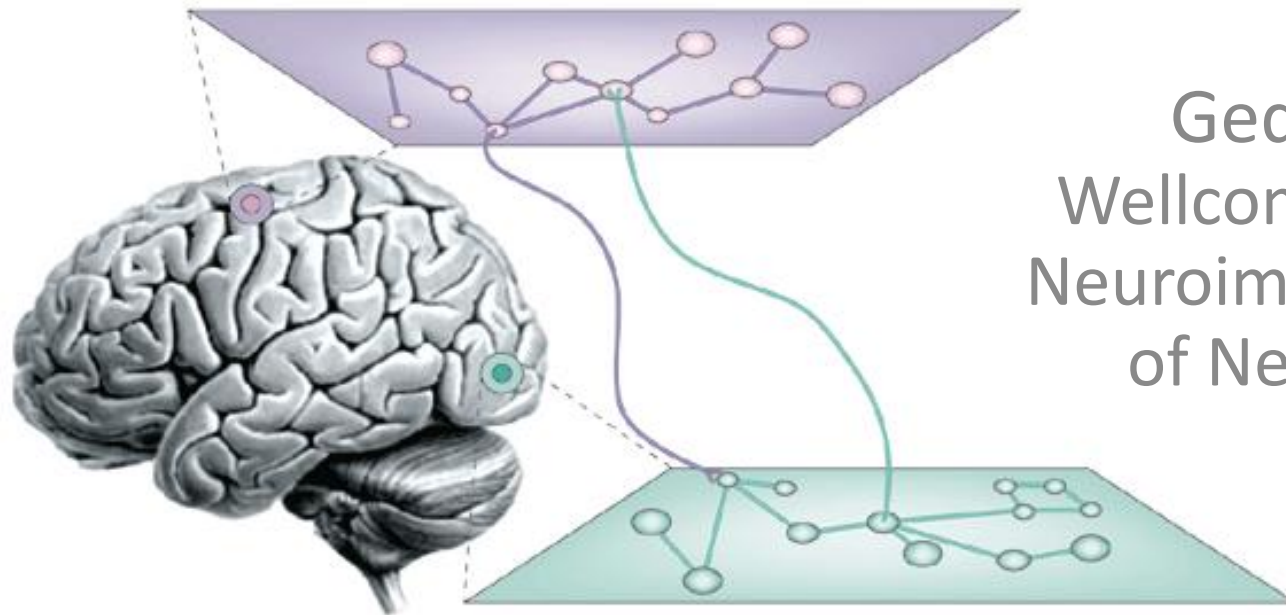


Stochastic Dynamic Causal Modelling for resting-state fMRI



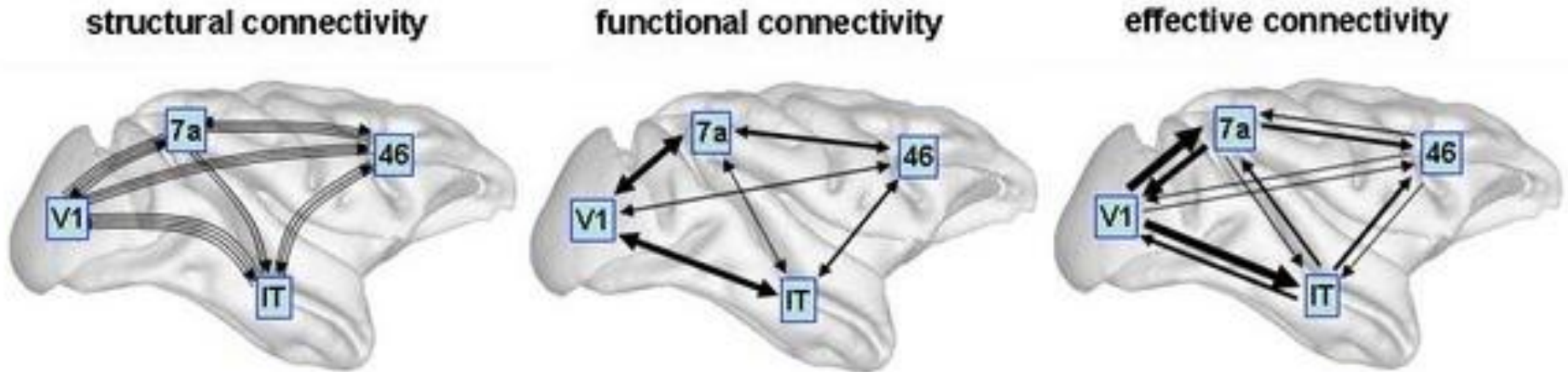
Ged Ridgway, FIL,
Wellcome Trust Centre for
Neuroimaging, UCL Institute
of Neurology, London

Overview

- Connectivity in the brain
- Introduction to Dynamic Causal Modelling
- Bayes, prior knowledge, and model evidence

- Connectivity in disease
- Motivation for resting-state fMRI in pharma
- Stochastic DCM and resting-state fMRI
- Pros and cons of sDCM for rs-fMRI in pharma

Connectivity in the brain

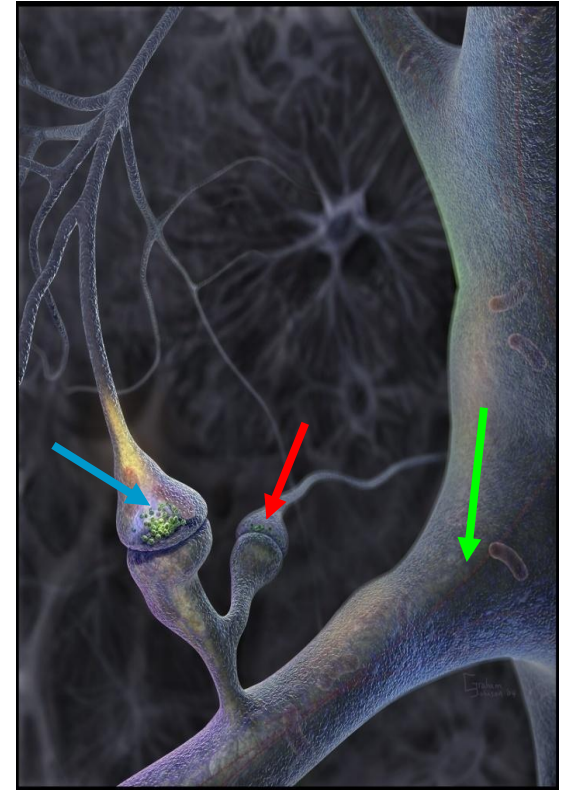


Sporns 2007, *Scholarpedia*

- **structural / anatomical connectivity**
= presence of axonal connections (from tracing or dMRI)
- **functional connectivity**
= statistical dependencies between regional time series
- **effective connectivity**
= causal (directed) influences between neuronal populations

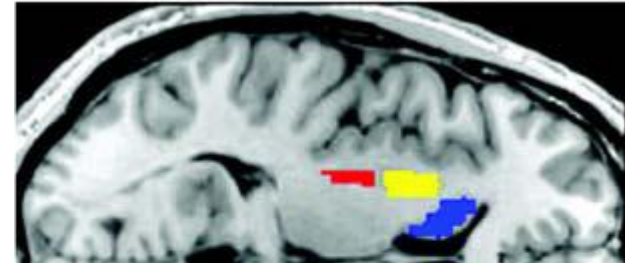
Functional and effective connectivity are dynamic

- Context-dependent recruitment and gating of connections
 - Synaptic depression over millisecc
 - Long-term potentiation over weeks
- Even structural connectivity changes
 - Microscopic and macroscopic (developmental) levels
 - (Friston, 2011, *Brain Connectivity*)
- Pharmacological manipulations

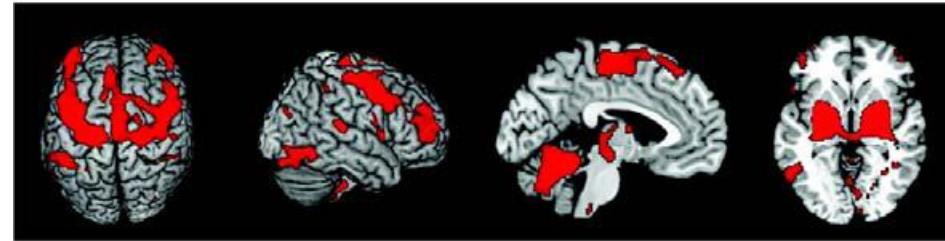


Analysis of functional connectivity

- Seed voxel correlation analysis
- Coherence analysis
- Eigen-decomposition (PCA, SVD)
- Independent component analysis (ICA)
- any technique **describing statistical dependencies** among regional time series



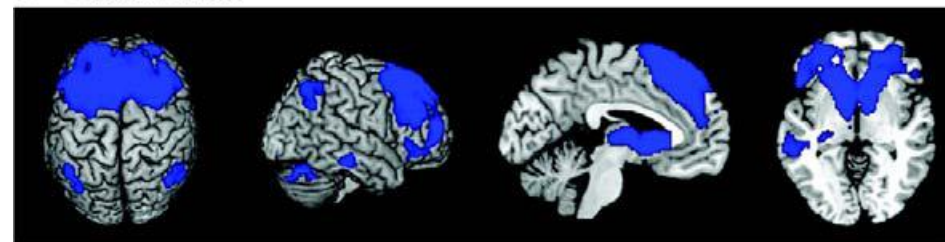
A Posterior Putamen



B Anterior Putamen



C Caudate Nucleus



Analysis of effective connectivity

- To get beyond descriptive statistical measures requires a model; parameterise connectivity
 - “modelling -> understanding”
- The model defines what is meant by (effective) direct/directed causal influence
- Model inversion yields estimated connectivity
- Generative models cause the observed data
 - “better to use an original than a derived measure”

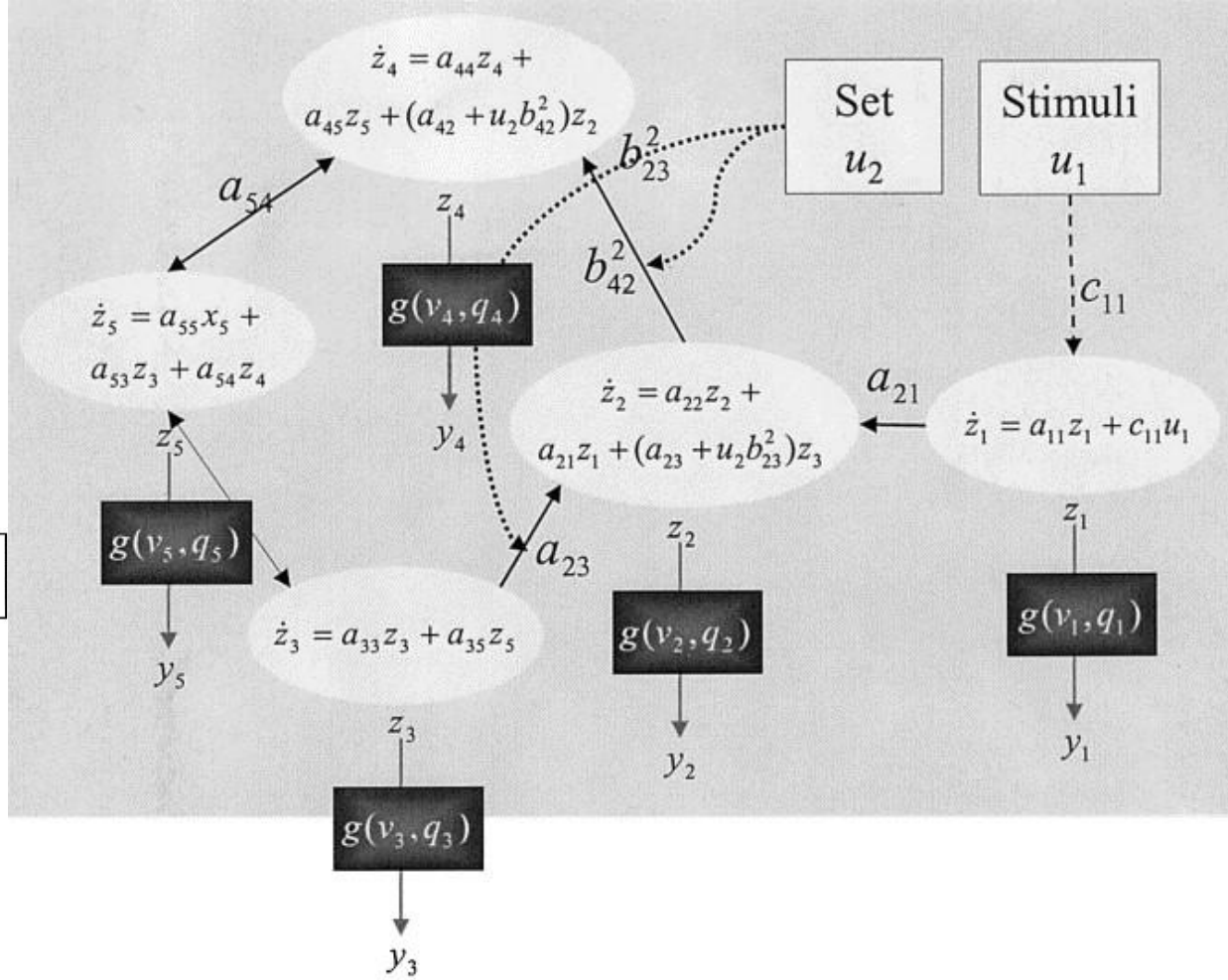
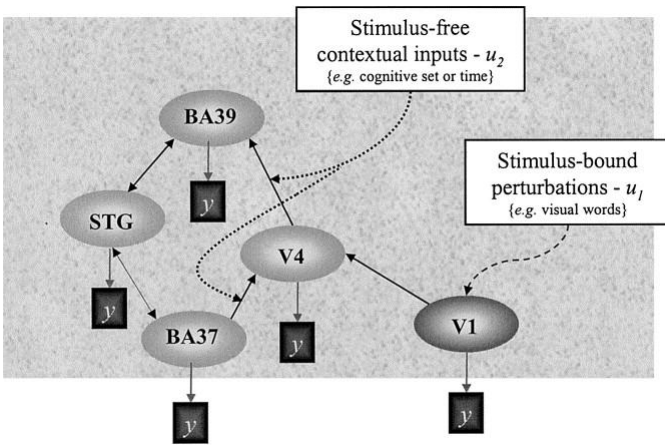
Generic time-series models

- Discrete-time “auto-regressive” models
 - next states = $f(\text{previous states, inputs, parameters})$
 - $x(k+1) = f(x(k), u, \theta)$
 - Underlies Granger Causality
 - Very roughly, if current x_1 and x_2 explain next x_1 better than x_1 does alone, then x_2 Granger-causes x_1
- Continuous-time dynamical systems models
 - rate of change = $f(\text{current states, inputs, parameters})$
 - $dx/dt = f(x(t), u, \theta)$
 - Used in Dynamic Causal Modelling
 - Bayesian model comparison **accounting for complexity**
 - Friston (2011) *Brain Connectivity*

Dynamic Causal Modelling

- Neurodynamic model (state evolution model)
 - Underlying (hidden) neuronal states \mathbf{x} (or often \mathbf{z})
 - $dx_i/dt = f(\{x_1, \dots, x_n\}, \{u_1, \dots, u_m\}, \{\theta_1, \dots, \theta_p\})$
 - Linear state-coupling terms: $a_{i1} x_1 + \dots + a_{in} x_n = \sum_k a_{ik} x_k$
 - Linear input terms: $c_{i1} u_1 + \dots + c_{im} u_m = \sum_j c_{ij} u_j$
 - Bilinear input-modulated coupling terms: $\sum_j \sum_k u_j B_{ijk} x_k$
 - $d\mathbf{x}/dt = \mathbf{A}\mathbf{x} + \mathbf{C}\mathbf{u} + \sum_j u_j \mathbf{B}^{(j)} \mathbf{x}$ [A, B and C in interface]
- Haemodynamic model (observation model)
 - Response = $f(\text{state, parameters}) + \text{confounds} + \text{noise}$
 - $y_i = g(x_i, \{ \theta_h \}) + \mathbf{X}\beta + \varepsilon$

DCM



$$\dot{z} = (A + \sum_j u_j B^j)z + Cu$$

The bilinear model

latent connectivity

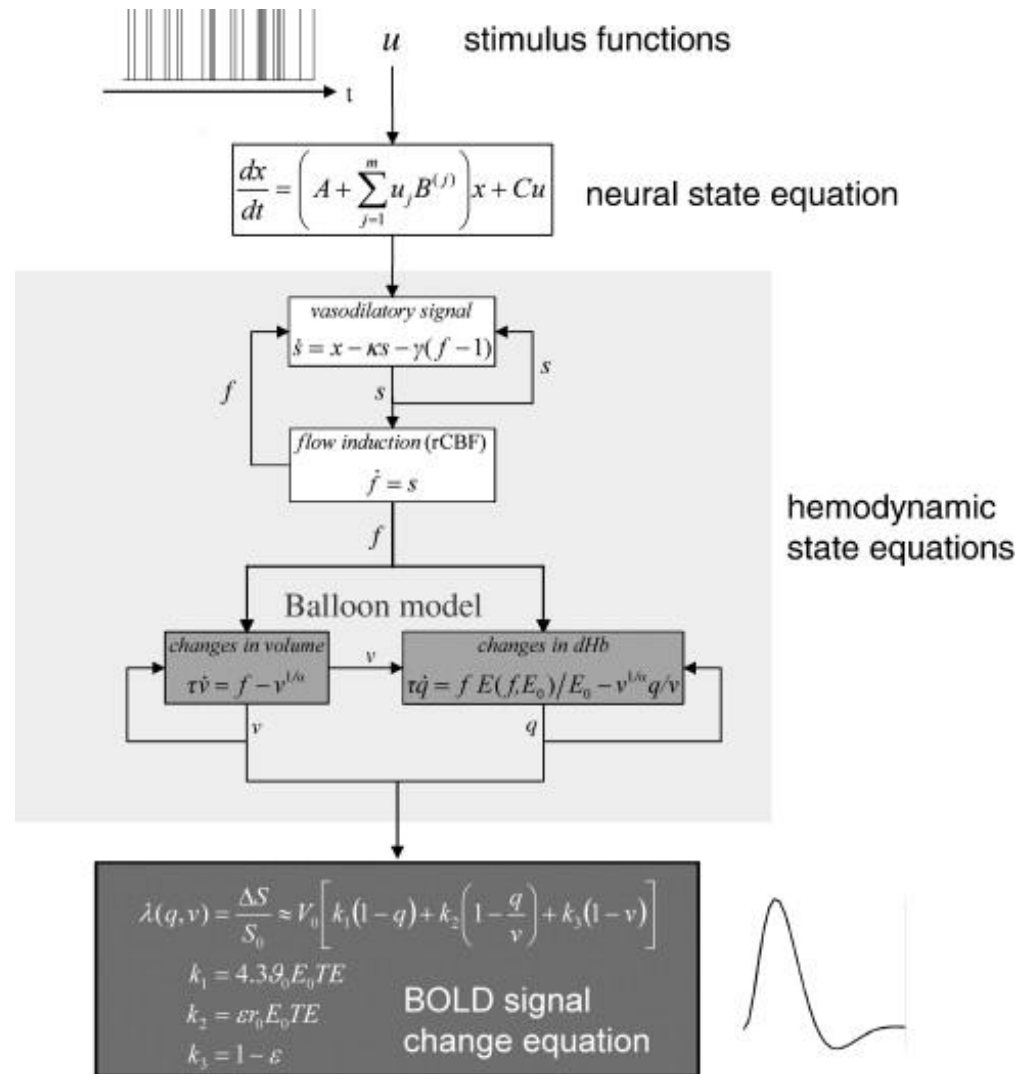
induced connectivity

$$\begin{bmatrix} \dot{z}_1 \\ \vdots \\ \dot{z}_5 \end{bmatrix} = \begin{bmatrix} a_{11} & \dots & 0 \\ a_{21} & a_{22} & a_{23} \\ \vdots & \vdots & a_{33} & a_{35} \\ 0 & a_{42} & a_{44} & a_{45} \\ \vdots & \dots & a_{53} & a_{54} & a_{55} \end{bmatrix} + u_2 \begin{bmatrix} 0 & \dots & 0 \\ \vdots & b_{23}^2 & \vdots \\ 0 & b_{42}^2 & \dots & 0 \end{bmatrix} \begin{bmatrix} z_1 \\ \vdots \\ z_5 \end{bmatrix} + \begin{bmatrix} c_{11} & 0 \\ \vdots & \vdots \\ 0 & 0 \end{bmatrix} \begin{bmatrix} u_1 \\ u_2 \end{bmatrix}$$

Forward, backward & self

DCM – haemodynamic model

- Generalises Buxton's balloon model
- Complete generative model including noise
- Bayesian inference allows prior constraints (& model comparison)
- Region specific
- Subject specific
- Treatment specific



DCM and Bayesian inference

- Generative or “forward” model (with noise distribution assumptions) gives “likelihood”:
 $p(\text{data} \mid \text{parameters, model})$
- To estimate parameters given observed data need to “invert” model:
 $p(\text{parameters} \mid \text{data, model})$
- Bayesian inference enables this inversion using “prior” information about parameters

Bayesian inference

- Bayes rule:
 - $p(A, B) = p(A | B) p(B) = p(B | A) p(A)$
 - **$p(B | A) = p(A | B) p(B) / p(A)$**
 - $p(A) = \sum_b p(A, B=b) = \sum_b p(A | B=b) p(B=b)$
- Bayes rule for DCM:
 - $p(\text{parameters} | \text{data}, \text{model})$
= $p(\text{data} | \text{parameters}, \text{model})$
x $p(\text{parameters} | \text{model})$
/ $p(\text{data} | \text{model})$

Bayesian model comparison

- The denominator, $p(\text{data} \mid \text{model})$, in turn gives $p(\text{model} \mid \text{data})$ via Bayes rule
- Allows computation of “Bayes factor” to compare $p(\text{model}_a \mid \text{data}) / p(\text{model}_b \mid \text{data})$
 - Note: same data; no absolute $p(\text{model}_a \mid \text{data})$
- Known as the model evidence and also the marginal likelihood, because parameters are marginalised / integrated out
 - Recall: $p(A) = \sum_b p(A, B=b)$
- Accounts for complexity (favours parsimony)

Bayesian model comparison

- Can be extended to encompass
 - Random effects model selection over subjects, allowing heterogeneity and outliers (Stephan et al. 2009, *NeuroImage*)
 - Bayesian parameter averaging and Bayesian model averaging accounting for uncertainty over models (Stephan et al. 2010, *NeuroImage*)
 - Comparison of families of models, e.g. top-down/bottom-up (Penny et al. 2010, *PLoS Comput Biol*)
 - Optimal experimental design (Daunizeau et al. 2011, *PLoS Comput Biol*)

Free energy in DCM (and the brain!)

- $p(\text{data} \mid \text{model}) = \int p(\text{data} \mid \theta, \text{model}) p(\theta) d\theta$
- However... the integration is impossible in practice
- We can optimise a lower bound on the model evidence known as the “free energy”
- Using “variational” calculus (variational Bayes)
- The optimised “proposal distribution” tends to the posterior distribution of interest
- Unlike other methods (e.g. Monte Carlo), could be implemented biologically – the Bayesian brain
 - (Friston, 2010, *Nat Rev Neurosci*)

Overview

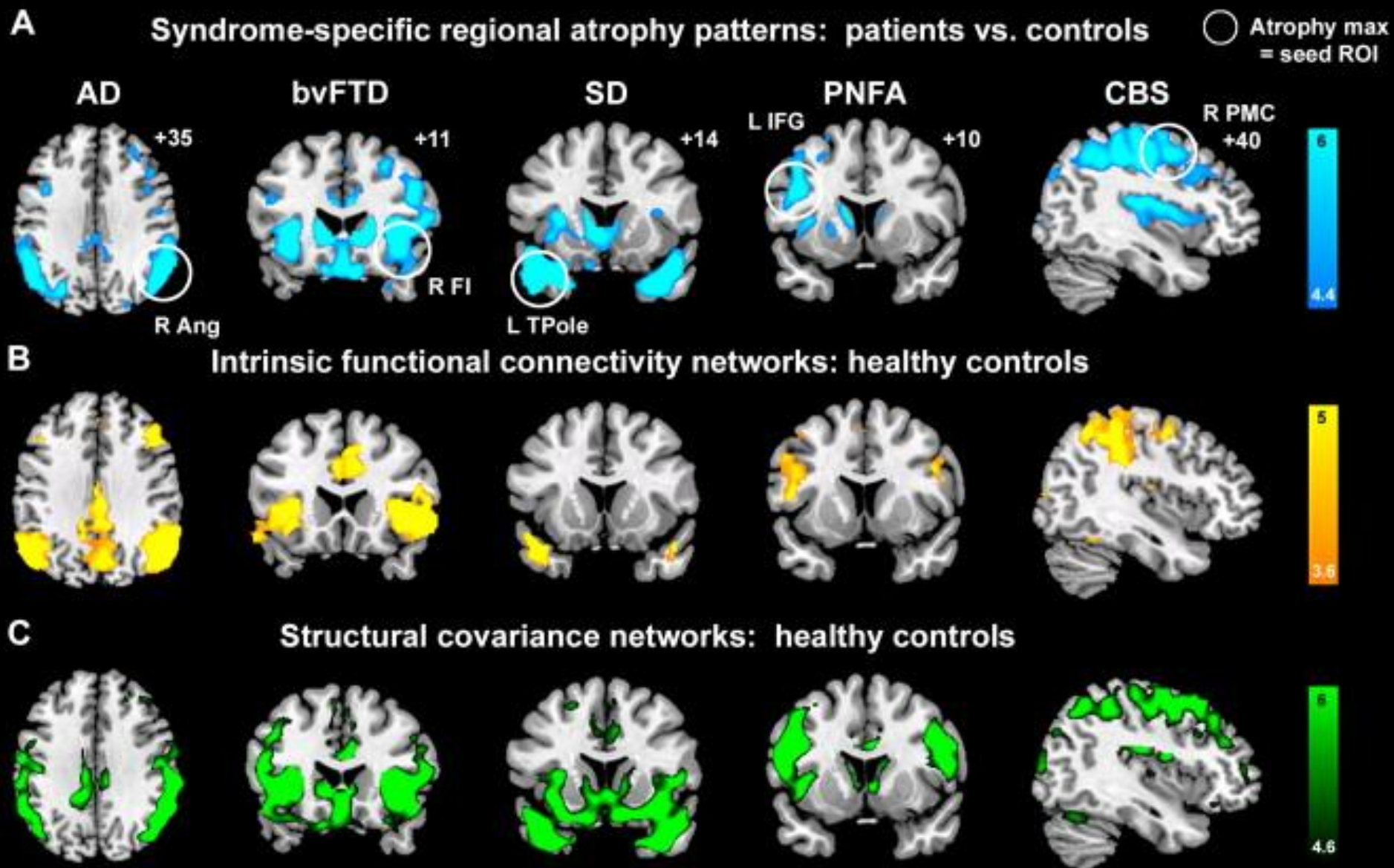
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Connectivity and disease

- “Dysconnection in Schizophrenia ...”
 - Stephan et al. (2009) *Schizophr Bul*
- “Autism spectrum disorders: developmental disconnection syndromes”
 - Geschwind et al. (2007) *Curr Opin Neurobiol*
- “Neurodegenerative Diseases Target Large-Scale Human Brain Networks”
 - Seeley et al. (2009) *Neuron*

Seeley et al. (2009)



Promising results / example applications

- Alzheimer's disease (and risk factors)
 - AD and MCI (Binnewijzend et al., in press, *Neurobiol Aging*)
 - Amyloid positive healthy elderly (Hedden et al., 2009, *J Neurosci*; Sheline et al., 2010, *Biol Psych*)
 - APOE e4 carrying elderly (Sheline et al., 2010, *J Neurosci*)
 - APOE e4 carrying under 35s! (Filippini et al., 2009, *PNAS*)
- Parkinson's disease
 - Rowe et al. (2010) *NeuroImage*:
 - “DCM model selection is robust and sensitive enough to study clinical populations and their pharmacological treatment”

Advantages of rs-fMRI for pharma

- Sensitivity to early/mild change
 - E.g. preceding structural atrophy
- Generality for multiple diseases and severities
 - No need for relevant (and implementable) task
 - No issue of task-difficulty, floor/ceiling effects, etc.
- Ease of standardisation, practicality
 - No special hardware or expertise required
 - Short scan, repeatable given problems

DCM for resting state data ?

- Neurodynamic model without inputs \mathbf{u}
- $d\mathbf{x}/dt = A\mathbf{x}$
- Stability requires (roughly) negative feedback
 - More precisely, negative real eigenvalues of A
- In the absence of input/perturbation \mathbf{x} decays
- Without dynamics of \mathbf{x} cannot have coupling!
- Require endogenous stochastic fluctuations
 - State noise – but differentiable rather than Markovian
 - $d\mathbf{x}/dt = A\mathbf{x} + \boldsymbol{\omega}$

Stochastic DCM

- Applicable to both task-driven and resting-state fMRI
- Uses variational Bayesian “generalised filtering” (Friston et al., 2010, *Math Probl Eng*)
- More complicated than usual state noise (cf. Kalman)
 - “separation of dynamics into a slow, low-dimensional flow on an attracting manifold and a fast (analytic) fluctuating part that describes perturbations”
 - “only the slow dynamics are communicated among nodes, which means we can model distributed activity with a small number of macroscopic variables (e.g. one per node) with fast fluctuations that are specific to each node” – (Friston et al., 2011, *NeuroImage*)

Regions/nodes for (s)DCM

- ROIs can come from prior hypotheses with anatomical atlases (though see “cons” later...)
- Or from functional connectivity analyses
 - E.g. distinct clusters from seed-correlation analysis
 - Or parts from ICA modes, or entire components from a high-dimensional ICA decomposition
- Nodes needn't be regions, can be distributed
 - E.g. distinct networks (such as default and exec.)
 - Note that (spatial) ICs can have dependencies...

sDCM of rs-fMRI for pharma – Cons

- Need for relatively strong hypotheses
 - Which ROIs, what topology, which aspects to test
- Definition of ROIs in individual subjects
 - Smith et al. (2011) *NeuroImage*, recommends against use of anatomical atlases for generic ROIs
 - Time-consuming, error-prone, less reproducible
- Validity of priors for pathology and/or drug
- Though all to some extent also cons for more general fMRI in pharma (assumptions = priors)

sDCM Cons – revisited

- Need for relatively strong hypotheses
 - + Savage-Dickey facilitates network discovery
- Definition of ROIs in individual subjects
 - + High-dimensional registration improving all the time (Dartel, LDDMM, ANTS, Nifty-Reg, Geodesic Shooting)
 - + Atlas fusion strategies can help (STAPLE, MAPS, LEAP)
- Validity of priors for pathology and/or drug
 - + Evaluating priors using model evidence (Moran et al.)

sDCM of rs-fMRI for pharma – Pros

- Connectivity from neuronal model parameters more interpretable than correlations or components; perhaps also more sensitive
- Potential for modelling concomitant neuronal and haemodynamic treatment effects
- Principled model selection, random effects inference (outliers, etc.), families of models
- Can be applied to regions within a network and/or to interacting networks
- Recent and on-going work enabling more nodes

Some useful references

- **The first DCM paper:** Dynamic Causal Modelling (2003). Friston et al. *NeuroImage* 19:1273
- **Physiological validation of DCM for fMRI:** Identifying neural drivers with functional MRI: an electrophysiological validation (2008). David et al. *PLoS Biol.* 6 2683
- **Hemodynamic model:** Comparing hemodynamic models with DCM (2007). Stephan et al. *NeuroImage* 38:387
- **Group Bayesian model comparison:** Bayesian model selection for group studies (2009). Stephan et al. *NeuroImage* 46:1004
- **Ten Simple Rules for Dynamic Causal Modelling** (2010). Stephan et al. *NeuroImage* 49(4):3099
- **Network discovery with DCM.** Friston et al., *NeuroImage* 56(3):1202
- Generalised filtering and **stochastic DCM** for fMRI. Li et al., *NeuroImage* 58(2):442